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<p>(54) Title: ANALYTICAL METHOD COMPRISING ADDITION IN TWO OR MORE POSITIONS AND A DEVICE AND TEST KIT THEREFOR</p> <div style="text-align: center; margin: 20px 0;"> $LZ_n \quad . \quad . \quad . \quad LZ_n \quad . \quad . \quad . \quad LZ_1 \quad \quad \quad DZ \quad \quad \quad (I)$ <p>-----></p> </div> <p>(57) Abstract</p> <p>A method and a device and test kit, respectively, for determination of an analyte in a sample in a flow matrix by means of a transport flow of one or more biospecific affinity reactants, at least one of which is analytically detectable (Reactant*) and one is firmly anchored in the matrix (Reactant I), have the characterizing features that: A. the flow matrix has at least two application zones for liquid (I) wherein a) LZ_n is an application zone for liquid, and n is the position of the application zone LZ_n, b) m is the total number of application zones in which flow is initiated ($m \geq 2$), c) one LZ_n is an application zone for sample ($LZ_n \cdot S$) and one LZ_n is for Reactant* ($LZ_n \cdot R^*$) with $n'' \geq n'$, d) -----> is the direction of the flow, e) DZ is the detection zone, and B. flow is initiated by adding liquid to each zone $LZ_m \dots LZ_n \dots LZ_1$ in such a way that liquid_{n+1}, added to the application zone LZ_{n+1}, is transported through the matrix immediately after liquid_n, added to the nearest downstream application zone LZ_n.</p>		

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ANALYTICAL METHOD COMPRISING ADDITION IN TWO OR MORE
POSITIONS AND A DEVICE AND TEST KIT THEREFOR

Technical field

5 The invention relates to a method for determination of an
analyte in a sample by use of biospecific affinity
reactants (Reactant 1, Reactant 2 etc.), one of which is
analytically detectable (Reactant*) and one is firmly
anchored in a detection zone in a transport flow matrix
10 (Reactant I). The sample (analyte) is transported by a flow
in the matrix from one application zone for liquid (LZS)
containing the analyte (sample) and/or a buffer, to the
detection zone (DZ), in which Reactant I is firmly
anchored. At the same time as the sample is transported in
15 the matrix the soluble reactants, including Reactant*, are
also being transported. In the detection zone Reactant* is
captured in an amount which is related to the amount of
analyte present in the sample. To achieve this, Reactant*
is chosen so that it may bind biospecifically directly to
20 Reactant I or indirectly via one or more added biospecific
affinity reactants (including the analyte). The amount of
analyte is then determined from the amount of Reactant*
bound in the detection zone. The transport flow may contain
zones, in which different biospecific affinity reactants
25 (e.g. Reactant*, but not analyte) have been applied in
advance (predeposited) in order to be dissolved and
transported along with the flow towards the detection zone.

By reactants (including the analyte), exhibiting
30 biospecific affinity (bioaffinity reactants), are meant
individual members in the reactant pairs: antigen/hapten -
antibody; biotin - avidin/streptavidin; two complementary
single chains of nucleic acid etc. As antibodies antigen
binding antibody fragments such as Fab, F(ab)₂, single
35 chain Fv antibodies (scFv) etc. are considered. Relevant
reactants do not have to be naturally occurring but can
also be synthetically produced molecules/binders.

The type of test methodology in question has previously been used primarily for biospecific affinity reactants where at least one part of an employed reactant pair has exhibited protein structure, in particular in connection with so called immunochemical determination processes.

The biospecific affinity reactions are primarily performed in aqueous media (e.g. water).

10

The technique in question is well known and has often been applied to so called test strips, where the strip has functioned as a flow matrix. The flow has been initiated in the zone to which the sample has been added (LZS). The flow has often been lateral, i.e. parallel to the surface of the matrix, or of other types, e.g. in depth in the matrix.

The test protocols have been of so called inhibition type (competitive) or non-inhibition type (non-competitive, sandwich). See e.g. Behringwerke US 4,861,711; Unilever WO 88/08534; Abbot US 5,120,643; Becton Dickinson EP 284,232 and US 4,855,240; Abbot/Syntex US 4,740,468; Pharmacia AB, WO 96/22532, etc.

In this context one often mentions simultaneous and sequential methods (protocols) regarding certain reactants (especially analyte and Reactant*). In simultaneous variants analyte (sample) and the relevant reactant, e.g. Reactant*, are transported simultaneously into the detection zone. Simultaneous variants may be obtained, if a sample is pre-incubated/mixed with Reactant* or if Reactant* has been predeposited in the sample application zone or in a zone downstream of the sample application zone but before the detection zone. In sequential variants the analyte (sample) is transported before a reactant, e.g. Reactant*, into the detection zone. Sequential variants may be obtained, if the relevant reactant, e.g. Reactant*, is added to the same application zone as the sample after the

sample (analyte) has been transported out of the zone. A variant of sequential methodology is discussed in US 4,855,240 (Becton & Dickinson). As an alternative to the sample (analyte) being transported before "tracer"

- 5 (=Reactant*) in the same transport flow, US 4,855,240 describes separated transport flows, in which the time of transport is regulated such that sample (analyte) reaches the detection zone before the "tracer" (Reactant*).
- 10 The term simultaneous tests has often included every variant, in which sample and Reactant* are pre-incubated/mixed before being added to a flow matrix or in which sample is added to a flow matrix, in which Reactant* is predeposited in the sample application zone or
- 15 downstream thereof. The term sequential tests has similarly included every variant, in which Reactant* is added to the sample application zone after the sample has migrated out of its application zone. Thus, considerations have not been taken, concerning if the order of analyte and Reactant* is
- 20 changed during transport to the detection zone. If not otherwise stated, this nomenclature is also used for the present invention, but is now adapted so that there are several application zones for liquid. This view means that primarily the initial order is considered, when both
- 25 analyte and Reactant* are in soluble form, and not the order in which analyte and Reactant* are transported into the detection zone.

Disadvantages with prior art and objects of the invention.

- 30 The prior art has often involved practical problems on automation, primarily because pre-incubation or sequential addition of sample and reactants have often been required, often in a certain predetermined order defined by the test protocol used. The object of the invention is to (a)
- 35 facilitate automation, (b) avoid sequential addition of sample and the analytically detectable reactant (Reactant*), and (c) allow for pre-deposited Reactant* when using sequential methodology, which relates to analyte and

Reactant*. More general aims are to achieve high quality test results, preferably with improved sensitivity and precision than given by previous variants.

5 The invention

Surprisingly we have now discovered that if flow is initiated by almost simultaneous addition of liquid to two adjacent zones in a flow matrix, the liquid added in the downstream zone migrates before the liquid which has been added in the upstream zone in direction towards the detection zone. Our discovery involves that zonewise migration of liquids may also be obtained if addition of liquid in an upstream zone is performed after addition of liquid in the nearest downstream zone. By applying this discovery on the relevant type of analysis methods, improvements can be obtained regarding the objects stated above.

A first main aspect of the invention relates to the initially mentioned analysis methods and is characterized in that

A. the flow matrix exhibits at least two application zones for liquid arranged substantially adjacent to each other:

25

$LZ_m \quad . \quad . \quad . \quad LZ_n \quad . \quad . \quad . \quad LZ_1 \quad \quad \quad DZ$
 ----->

wherein

- 30 a) LZ_n is an application zone for liquid, where n is the position of the application zone LZ_n (n is an integer $2 < n \leq m$)
- b) m is the total number of application zones, in which flow is initiated,
- 35 c) one LZ_n is an application zone for sample (LZ_n, S) and one $LZ_{n'}$ is application zone for Reactant* ($LZ_{n'}, R^*$) with $n'' \geq n'$,

- d) -----> is the direction of the flow, and
 e) DZ is detection zone, and

B. flow is initiated by adding liquid to each zone

- 5 $LZ_m . . . LZ_n . . . LZ_1$ in such a way that liquid_{n+1}, added to the application zone LZ_{n+1} , is transported through the matrix after liquid_n, added to the nearest downstream application zone LZ_n .
- 10 Liquid_{n+1} may easily migrate immediately after liquid_n, if the corresponding zones for application of liquid are adjacent to each other or if added liquid volumes are adapted for this aim.
- 15 In the most common case the above mentioned involves adding liquid_{n+1} to LZ_{n+1} before or primarily simultaneously with adding liquid_n to LZ_n . For $n = m$, LZ_{n+1} is lacking, and for that zone it is therefore not possible to add any liquid to LZ_{m+1} . Practical advantages are achieved if the addition is
- 20 performed primarily simultaneously for all $LZ_m . . . LZ_n . . . LZ_1$.

- The number (m) of application zones for liquid ($LZ_m . . . LZ_n . . . LZ_1$) may in principle be any number with
- 25 the exception of one ($m \neq 1$). For practical reasons it is likely that in the future $2 \leq m \leq 10$, preferably $2 \leq m \leq 6$, such as $m = 2$ or 3 or 4 or 5 .

- The liquids added (liquid₁ . . . liquid_m) may consist of
- 30 only buffer solution or buffer solution plus a reactant (Reactant 1, Reactant 2 etc.), needed to make it possible for Reactant* to be captured in the detection zone in an amount related to the amount of analyte in the sample. Also Reactant* may be included in a liquid_n. As a rule the
- 35 composition of transported components from an application zone is not the same as from the nearest adjacent application zone, in which flow is initiated (LZ_{n+1} and LZ_{n-1}

with the exception of $n = m$ and $n = 1$ for which the zones LZ_{n+1} and LZ_{n-1} , respectively, are lacking).

By the expression "substantially adjacent to each other" is meant that the application zones for liquid are immediately adjacent to each other or with an intermediate area of matrix which preferably is no more than about 2 mm, and particularly no more than about 1 mm.

10 A liquid added in an application zone may have a tendency to spread on top of the matrix to parts of the matrix being outside the zone. For adjacent zones this means that liquids may be mixed with each other in an undesired way. To avoid this, physical barriers delimiting two adjacent
15 application zones (zone spacers) are placed. The barriers should primarily be placed on top of the matrix, but may be extended down into the matrix without completely quenching the flow. Delimitation is primarily against an adjacent zone for application of liquid, but can of course extend
20 around a whole application zone for liquid. Liquid may also be introduced via pads or material layers applied on the matrix and from the same or a different material than the matrix material. In such a case there is no need for zone spacers.

25 Relevant reactants may be predeposited in an application zone for liquid (LZ_n) or between two such zones. An application zone for liquid, only intended for transporting buffering components and/or other components not
30 participating in the biospecific affinity reactions (i.e. liquid neither containing nor intended for transport of any reactant or analyte), is called LZ_nB below. An application zone for liquid (LZ_n), where the liquid contains a reactant or is intended for transport of a reactant, e.g. Reactant*,
35 Reactant 1, Reactant 2 etc., is called LZ_nR^* , LZ_nR1 , LZ_nR2 etc. below. If a liquid_n is to transport a combination of components, e.g. Reactant* and analyte (sample) the application zone will be common for the

components and will be designated $LZ_n \dots R2/R1$ etc. For the combination sample and Reactant*, the application zone will be $LZ_n, R^*/S$ ($n' = n''$). That liquid_n is intended for transport of a certain reactant includes that the reactant in question also can be predeposited in the zone LZ_n . The latter includes that the reactant may be predeposited in an area downstream of the application zone for the relevant liquid but upstream of the nearest downstream located LZ (LZ_{n-1}), or if $n = 1$ only upstream of the detection zone (as LZ_{n-1} then is lacking).

By predeposition is meant that a reactant is added in advance to the matrix and in a way so as not to spread in the matrix until it is reached by liquid, which has been applied to initiate flow. Predeposition of reactants may be performed in a way known per se. (See e.g. Behringwerke US 4,861,711; Unilever WO 88/08534; Abbot US 5,120,643; Becton Dickinson EP 284,232). It is important that arrangements are made so that the reactant in question is quickly dissolved, when liquid passes through an area, containing predeposited reactant. In order to achieve quick dissolution it has been common to incorporate reactants in substances that as such dissolve quickly. This type of substances are often hydrophilic with polar and/or charged groups, such as hydroxy, carboxy, amino, sulphonate etc. In particular there may be mentioned hydrophilic quickly soluble polymers, e.g. having carbohydrate structure, simple sugars including mono-, di- and oligosaccharides and corresponding sugar alcohols (mannitol, sorbitol etc.). It is common practice to first coat the application zone in question with a layer of the quickly soluble substance, and then the reactant is applied, optionally followed by one additional layer of quickly soluble substance. An alternative way is by incorporating the reactant in particles of quickly soluble material which then are deposited in the relevant zone of the matrix.

- Some of the most important embodiments regarding the application zones for liquid may be summarized: $2 \leq m \leq 6$; n' is 1, 2 or 3; $n'' > n'$ or $n'' = n'$; $LZ_{n,S}$ is the application zone for sample and optionally also for
- 5 Reactant* or other reactant; $LZ_{n'+1}$, $LZ_{n'+2}$, $LZ_{n'+3}$, $LZ_{n'-1}$, and $LZ_{n'-2}$ are application zones for liquids intended for transport of Reactant* or other reactant or buffer without reactant as far as allowed by m , n'' and n' .
- 10 Transport flow through the particular types of matrix may be achieved by the action of capillary forces, e.g. by starting with a substantially dry matrix. A sucking body may be placed at the end of the flow as an aid. Flow, meaning transport of primarily only dissolved components,
- 15 may be achieved if an electrical field is applied across the matrix.

Test protocols

- By use of the invention reactants and analyte can be made
- 20 to migrate zonewise as individual components or together in different combinations towards the detection zone. The exact sequence of application zones is determined by the test protocol to be utilized.
- 25 The invention may be applied to competitive (inhibition) as well as non-competitive (non-inhibition) test variants irrespective of if these are simultaneous or sequential regarding any reactant. Illustrative systems are shown schematically below in form of the complexes formed. "-"
- 30 relates to firm anchoring to the matrix, "---" relates to binding via biospecific affinity. For the sake of simplicity it has been assumed that reactants used are monovalent regarding utilized binding sites.

A. Sandwich protocol (non-inhibition)

Reactant I and Reactant* both have biospecific affinity for the analyte. x = number of moles of Reactant I on the matrix and y = number of moles of analyte (= number of moles of Reactant*), bound to Reactant I.

Complex in the detection zone:

Matrix $(\text{-Reactant I})_{x \cdot y}$ $(\text{-Reactant I --- analyte --- Reactant*})_y$

10

Simultaneous variants:

$m = 2$: $\text{LZ}_2\text{R}^*/\text{S}$ LZ_1B DZ

Sequential variants:

15 $m = 2$: LZ_2R^* LZ_1S DZ .

$m = 3$: LZ_3R^* LZ_2B LZ_1S DZ and alternatives where the buffer zone has position 1 or 3.

$m = 4$: LZ_4B LZ_3R^* LZ_2B LZ_1S DZ and alternatives where any of the buffer zones is placed in position 1.

20 $m = 5$: The same sequence as for $m = 4$ with the exception that an extra buffer zone is placed in position 1.

B. Sandwich protocol (non-inhibition):

Reactant I exhibits biospecific affinity for Reactant II.

25 Both Reactant II and Reactant* have biospecific affinity for the analyte. x = number of moles of Reactant I on the matrix, y = number of moles of analyte (= number of moles of Reactant*), bound to Reactant I via Reactant II. $y + z$ is the number of moles of Reactant II bound to Reactant I.

30

Complex in the detection zone:

Matrix $(\text{-Reactant I})_{x \cdot z \cdot y}$ $(\text{-Reactant I --- Reactant II})_z$ $(\text{-Reactant I --- Reactant II --- analyte --- Reactant*})_y$

35 Simultaneous variants:

$m = 2$: The same as for protocol A with the exception that $\text{LZ}_2\text{R}^*/\text{S}$ is $\text{LZ}_2\text{R}^*/\text{S}/\text{RII}$ or that LZ_1B is LZ_1RII .

$m = 3$: $\text{LZ}_3\text{R}^*/\text{S}$ LZ_2B LZ_1RII DZ or

LZ₃R*/S LZ₂RII LZ₁B DZ.

Sequential variants:

m = 2: The same as for protocol A with the exception that

5 LZ₁S is replaced by LZ₁S/RII.

m = 3: LZ₃R* LZ₂B LZ₁S/RII DZ or

LZ₃R* LZ₂S LZ₁RII DZ or

LZ₃R* LZ₂S/RII LZ₁B DZ.

m = 4, 5, 6: In analogy with protocol A sequences with up
10 to 6 application zones for liquid may be considered.

C. Inhibition protocol:

Reactant I is an analyte analogue, firmly anchored to the matrix, Reactant III exhibits biospecific affinity for the
15 analyte and Reactant* has biospecific affinity for Reactant III. x = number of moles of Reactant I on the matrix. y = number of moles of Reactant III (= number of moles of Reactant*), bound to the matrix via Reactant I. The conditions are selected so that y is a measure of the
20 amount of analyte in the sample.

Complex in the detection zone:

Matrix (-Reactant I)_{x-y} (-Reactant I --- Reactant III ---
Reactant*)_y

25

Simultaneous variants:

m = 2: LZ₂R*/RIII/S LZ₁B DZ.

Sequential variants:

30 m = 2: LZ₂R* LZ₁/RIII/S DZ.

m = 3, 4 and 5: May be built up in analogy with protocol A.

D. Inhibition protocol

Reactant I exhibits biospecific affinity for both Analyte
35 and Reactant*. Reactant* is a soluble analyte analogue. x + y is the number of moles of Reactant I on the matrix, x and y are the number of moles of Reactant* and Analyte, respectively, being bound to the matrix.

Complex in the detection zone:

Matrix (-Reactant I --- Reactant*)_x (-Reactant I ---
Analyte)_y:

5

Simultaneous variant:

m = 2: LZ₂R*/S LZ₁B DZ

Sequential variant:

10 m = 2: LZ₂R* LZ₁S DZ

m = 3, 4 and 5 may be built up in analogy with protocol A.

Matrices

The matrix defines the space in which the flow is
15 transported. The matrix may be the inner surface of a
simple flow channel (e.g. a capillary), the inner surface
of a porous matrix having a system of flow channels (porous
matrix) etc. extending through. For the sake of simplicity,
matrices, usable in this variant of the invention, will be
20 called flow matrices. Porous matrices may exist in the form
of monoliths, sheets, columns, membranes, single flow
channels having capillary dimensions or aggregated systems
of such flow channels etc. They may also exist in the form
of particles packed in column casings, compressed fibres
25 etc. The inner surface of the matrices, i.e. the surface of
the flow channels, should be hydrophilic, such that aqueous
media (usually water) may be absorbed and transported
through the matrices. The smallest inner dimension of the
flow channels should be sufficiently large for allowing
30 transport through the matrix of the reactants being used.
The rule of thumb is that suitable matrices are selected
among those having flow channels with the smallest inner
dimension (often as a diameter for round channels) in the
interval 0.4-1000 µm, preferably 0.4-100 µm if the matrix
35 exhibits a system of mutually communicating flow channels.
Flow channels having a smallest inner dimension in the
upper part of the interval 0.4-1000 µm are primarily of

interest for simple unbranched channels, through which flow is driven by an externally imposed pressure or suction.

Relevant matrices are often built up from a polymer, e.g. nitrocellulose, nylon etc. The material in the matrix as well as the physical and geometrical design of the flow channels may vary along the flow depending on what a certain part of the matrix is to be used for (Pharmacia AB WO 96/22532; Medix WO 94/15215).

10

Detection zone

In the detection zone, Reactant I is firmly anchored to the matrix with bonds not allowing unintentional transport of Reactant I under the test conditions. Attachment of

15 Reactant I to the matrix may be covalent, via physical adsorption, via biospecific affinity etc. Like prior art in this field the invention may utilize combinations of binding types, e.g. covalent binding to the matrix of a biospecific affinity reactant directed to Reactant I. In

20 particular may be mentioned a matrix exhibiting a physically adsorptively or covalently bound member of a specific binding pair (reactant pair) in combination with Reactant I coupled or conjugated to the other member of the specific binding pair, or a matrix exhibiting a similarly

25 bound antibody directed to Reactant I. As examples of specific binding pairs may be mentioned immunological binding pairs, such as antigen-antibody and hapten-antibody, biotin-avidin or -streptavidin, lectin-sugar, hormone-hormone receptor, nucleic acid duplex. If reactant

30 I binds to the matrix via another reactant according to the above, Reactant I need not be immobilized in the matrix but may either be movably (diffusively) predeposited in the matrix in an area or zone that is separated from the detection zone, or it may be added together with or

35 separately from the sample. Anchoring of Reactant I to the matrix may be achieved via particles having been deposited in/on the matrix and to which Reactant I is covalently, physically adsorptively or biospecifically etc. bound. The

particles attach to the matrix either because their size has been selected such that they cannot be transported through the matrix or via physical adsorption. See inter alia Abbott/Syntex US 4,740,468; Abbott EP 472,376;

5 Hybritech EP 437,287 and EP 200,381; Grace & Co. EP 420,053; Fuji Photo Film US 4,657,739; Boehringer Mannheim WO 94/06012. For the invention the latter variant with smaller particles adsorbing physically to the matrix has been shown to be good.

10

In one and the same transport flow there may be several detection zones (DZ1, DZ2 etc.). One or more of the detection zones may relate to the same or different analytes. If the analytes are different Reactant I is

15 usually different for each DZ.

Analytically detectable reactant (Reactant*)

In the invention Reactant* cannot be an analyte. Usually analytical detectability is obtained because a natural

20 reactant, e.g. an antibody or an antigen or a hapten, is provided with an analytically detectable group. Well known examples of often used groups are enzymatically active groups (enzyme, co-factor, co-enzyme, enzyme substrate etc.), fluorogenic, chromophoric, chemiluminiscent,

25 radioactive groups etc. Groups being detected by means of a biospecific affinity reactant usually also are referred to this category, e.g. biotin, hapten, class-, subclass- and species-specific determinants in immunoglobulins etc.

30 A preferred label group is particles optionally containing any of the detectable groups above, such as fluorophoric groups or chromogenic groups (coloured particles). Useful particles often have a size in the interval of 0.001-5 μm . The particles may have colloidal dimensions, so called sol
35 (i.e. usually spherical and monodisperse having a size in the interval 0.001-1 μm). Especially metal particles (e.g. gold sol), non-metal particles (e.g. SiO_2 , carbon, latex

and killed erythrocytes and bacteria) may be mentioned. Also particles of non-colloidal dimensions but with focus on non-sedimenting capability have been used. These have been more or less irregular and more or less polydisperse

5 (carbon particles < 1 μ m; Pharmacia AB, WO 96/22532).

For particles as label group reference is made to Unilever WO 88/08534; Abbott US 5,120,643; Becton Dickinson EP 284,232 among others.

10

In connection with the development that has led to the present invention it was surprisingly found that good results may be obtained if one simultaneously utilizes:

15 (a) Reactant* with label particles according to the above as a detectable group, and

(b) a detection zone, in which Reactant I has been anchored to the matrix via particles substantially having dimensions that would allow transport of the
20 particles as such through the matrix.

We have achieved functioning systems, in which label particles and anchoring particles substantially have the
25 same dimensions. This means with great probability that the label particles may be larger than the anchoring particles and vice versa, as long as they remain smaller than the flow channels defined by the matrix. The system may function with or without pre-deposition of Reactant* in the
30 intended application zone. This embodiment is part of an invention, described in our co-pending PCT application: "Analytical method using particles and test kit for performing the method" (based on SE 9704935-7). This separate patent application is incorporated herein by
35 reference.

Analytes

The invention is primarily adapted for determination of biospecific affinity reactants of the types initially mentioned. The reactants may be a cell or a virus or a part thereof. In particular antigen, such as an immunoglobulin or an antibody may be mentioned. For immunoglobulins the determination may relate to a certain Ig and/or certain Ig subclass. For antibodies the determination may relate to a certain specificity, optionally also the Ig class or the Ig subclass of the antibody. Relevant Ig classes are IgA, IgD, IgE, IgG and IgM. Relevant Ig subclasses are IgG1, IgG2, IgG3 and IgG4.

In sandwich variants (according to protocols A and B, above) the analyte may be an antibody, directed to an allergen/antigen/hapten and be derived from a certain species, a certain Ig class or a certain Ig subclass. In this case Reactant* may be an analytically detectable antibody directed to an epitope specific for the species, Ig class or Ig subclass and with Reactant I (protocol A) or Reactant II (protocol B) as the allergen/antigen/hapten. Alternatively the reverse may be selected, i.e. Reactant* is the allergen/antigen/hapten and Reactant I and Reactant II, respectively, is the antibody, directed to the analyte. When the analyte is an antigen in general, both Reactant I and Reactant* may be antibodies, directed to the antigen, in protocol A. For protocol B it is Reactant II and Reactant* that are antibodies directed to the antigen.

Competitive variants are most interesting for low molecular analytes. Illustrative examples are antigen and hapten. For protocol C Reactant I may be the antigen or the hapten, firmly anchored to the matrix, Reactant III may be an antibody, directed to the antigen, and Reactant* may be an antibody, directed to Reactant III. For protocol D Reactant I may be an antibody directed to the analyte and Reactant* may be the analyte labelled with an analytically detectable group.

The method of the invention may be performed as part of diagnosing allergy or autoimmune disease.

- 5 For the inventors it has been of special interest to measure anti-allergen antibodies of IgE or IgG class, for the latter preferably with focus on any of the subclasses mentioned. Measuring of allergen-specific antibodies can be utilized when diagnosing IgE mediated allergy.

10

Samples

- Relevant samples may be of biological origin, e.g. from different body fluids (whole blood, serum, plasma, urine, saliva, tear fluid, cerebrospinal fluid etc.), from cell
15 culture media, processing procedures in biotechnology, from tissue extracts, from food stuff, from the environment (environmental analysis samples) etc. The samples may be pretreated in order to fit e.g. the matrix, the test protocol involved etc.

20

Calibrators

- Determination methods of the type that the invention is related to, involve that the detectable signal from the analytically detectable reactant (Reactant*) is measured
25 and the measured signal (sample value) is taken as a measure of the amount of analyte present in the sample. To transfer the measurement signal to actual amounts of analyte the signal is usually compared to the corresponding signal (calibrator value) of known standard amounts of
30 analyte (calibrators). In connection with the present invention a new calibrator system has been developed, which applied to the present invention constitutes a best embodiment.

- 35 This separate invention means that the used calibrator in advance has been anchored to a matrix (matrix calibrator), preferably of the same type as the one utilized for sample run. When measuring calibrator values, matrix calibrator is

allowed to bind to Reactant*, and then the measurement signal from Reactant* is measured in a way known per se. By utilizing different amounts of matrix calibrator a series of calibrator values may be obtained corresponding to
5 different pre-determined amounts of analyte in sample (standard amounts, dose-response curve, calibration curve).

Alternatively, instead a binder for the calibrator has been anchored to the matrix, and calibrator is added at the
10 determination of calibrator value, optionally pre-deposited in the matrix upstream of the calibrator zone(s) to be dissolved by sample solution or buffer at the determination. When a calibrator binder is bound to the matrix, the calibrator may either be movably (diffusively)
15 pre-deposited in the matrix in a zone separated from the detection zone, or be added together with or separately from the sample. The calibrator binder is usually one member of a specific binding pair (reactant pair), the other member of the binding pair being coupled or
20 conjugated to the calibrator substance. As examples of such specific binding pairs may be mentioned immunological binding pairs such as antigen-antibody and hapten-antibody, biotin-avidin or -streptavidin, lectin-sugar, hormone-hormone receptor, nucleic acid duplex.

25 Applied to the present invention our new calibrator system involves primarily that the transport flow passes one or more zones with a calibrator, firmly anchored to the matrix in the respective calibrator zone (CZ).

30 Anchoring of a calibrator to the matrix in a calibrator zone may be performed according to the same principles as for anchoring of Reactant I to a detection zone.

35 Calibrator zones should be located downstream of an application zone for liquid, intended for transport of Reactant*. In relation to the detection zone (DZ) the calibrator zone is preferably located upstream.

Our invention relating to calibrators is described in detail in our co-pending PCT application with the title "Method using a new calibrator and a device and test kit including the calibrator" (based on SE 9704933-2). This application is incorporated herein by reference.

A second main aspect of the invention

The flow matrix according to the above containing two or more application zones for liquid, optionally in the form of a kit wherein the flow matrix is comprised together with the analytically indicatable reactant, constitutes a second main aspect of the invention.

The invention is illustrated in the following non-limiting experimental part.

EXAMPLE 1: SEQUENTIAL METHOD WITH THE ZONE SEQUENCE: LZ₄B, LZ₃R*, LZ₂B, LZ₁S, DZ. DETECTION OF hIgE IN TEST VARIANT WITH CARBON PARTICLE CONJUGATE

Methods and materials

Adsorption of phenyldextran to polystyrene particles:

Phenyldextran (substitution degree: 1 phenyl group on each fifth monosaccharide unit = 20%, Mw dextran 40,000, Pharmacia Biotech AB, Uppsala, Sweden) was adsorbed to polystyrene particles (0.49 µm Bangs Laboratories, USA) by incubations under stirring with phenyldextran dissolved in deionized water to 1) 5 mg/ml, 10% particle suspension, RT 30-60 minutes; 2) 5 mg/ml, 5% particle suspension, RT 1 h; 3) 20 mg/ml, 1-2% particle suspension, RT 3 h or overnight. The particles were subsequently washed twice with deionized water. The particle suspensions were centrifuged between each incubation and wash (12,100xg, 25 min, Beckman, J-21, JA-20, 10,000 rpm). The particle suspension was finally sonicated (Ultrasonic bath, Branson 5210, 5 min).

Coupling of anti-human IgE antibody (anti-hIgE) to

polystyrene particle: Anti-hIgE was coupled to phenyldextran coated polystyrene particles with CDAP (1-cyano-4-dimethylamino-pyridinium bromide (Kohn J and

5 Wilchek M, FEBS Letters 154(1) (1983) 209-210).

Desalting and change of buffer of anti-hIgE was performed by gel filtration (PD-10, Pharmacia Biotech AB) in NaHCO_3 , 0.1 M, pH 8.5. 2.3 g of polystyrene particles (coated with
10 phenyldextran according to above) in 2% solution in 30% (by volume) acetone were activated with 17 ml CDAP (0.44 M) and 14 ml TEA (0.2 M triethylamine, Riedel-deHaën, Germany). CDAP was added with stirring for 150 seconds and TEA for 150 seconds. The particles were washed with 30% (by volume)
15 acetone and centrifuged at 12,100xg (25 min, Beckman, J-21, JA-20, 10,000 rpm). 17 of anti-hIgE was coupled to the activated particles (2%, 0.15 g in 0.1 M NaHCO_3 , pH 8.5) in incubating with stirring overnight at +4°C. The particles were centrifuged and decanted before deactivating with
20 glutamic acid 0.05 M and aspartic acid 0.05 M in 0.1 M NaCHO_3 , pH 8.5 when incubating with stirring overnight at +4°C. Coupled particles were washed once with 0.1 M NaHCO_3 , 0.3 M NaCl , pH 8.5, once with 0.1 M HAc , 0.3 M NaCl pH 5, once with 0.1 M NaHCO_3 , pH 8.5 and once with 20 mM borate
25 buffer pH 8.5.

The concentration of particles was determined spectrophotometrically at A_{600} nm with untreated particles as reference. Concentration of coupled protein was
30 determined by having anti-hIgE present during the coupling and cpm measurement.

Carbon particle conjugate (Reactant*): This was prepared by anti-hIgE being adsorbed to carbon particles (sp100, < 1
35 μm , Degussa, Germany) according to WO 96/22532 (Pharmacia AB). The final solution used in the flow matrix contained 400 μg of carbon particles per ml.

Deposition of anti-hIgE-coupled particles on membrane: On nitrocellulose sheets (Whatman, 8 μ m, length 5 cm and width 25 cm with polyester backing, anti-hIgE particles (prepared according to the above) were deposited in a zone over the width of the sheet (future detection zone) with Linear Striper (IVEK Corporation). The flow was 1 μ l/sec and 1 μ l/cm. The particles were diluted in borate buffer (20 mM, pH 8.5, Dextran T5000 4.2% w/w, sorbitol 5.8% w/w). The amount of deposited anti-IgE antibody was about 1000 ng/cm. The sheets were dried for 1 h at 30°C.

Zones for application of buffer, sample and carbon particle conjugate: Well separated from the zone, containing deposited material, 4 Inplastor strips (Mylar with glue on one side, Gelman) with a width of 1 mm were placed in parallel with the zone and parallel with each other at a distance of 5 mm from each other (zone spacers). The Inplastor strips thus defined four zones with a width of 5 mm. The sheets were cut perpendicularly relative to the zone containing deposited material, to strips with a width of 0.5 cm (the length of the strip then became 5 cm) (Singulator: Matrix 1201 membrane cutter, Kinematic automation). The final strips exhibited four parallel zones (application zones) separated by Inplastor strips as zone spacers and a separate zone with deposited anti-hIgE antibody (detection zone). As a comparison strips without zone spacers, i.e. without separated application zones were produced.

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Test methodology: Strips with separated application zones were mounted on a plane holder. At the top (0.5 cm) of the strip (and with the detection zone as the nearest zone) a sucking membrane was placed (Whatman, 17 Chr, width 3 cm). The holder also gave a constant pressure on the sucking membranes. For simultaneous application of reagents to the four subzones a 4 channel Multipipette (Labsystems) was

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used. The multipipette was loaded so that serum sample (30 μ l) was applied in the application zone nearest to the detection zone in the order of buffer (30 μ l), carbon particle conjugate (30 μ l) and buffer (30+30 μ l) in the
5 respective upstream application zone. For sequential application to the strips without zone spacers, 30 μ l of sample were first applied to the lower end of the strip. After suction of sample volume, buffer (30 μ l), carbon particle conjugate (30 μ l) and buffer (30+30 μ l) were added
10 successively after suction. The carbon particle conjugate was prepared according to above and suspended in buffer. The buffer was NaPO_4 0.1 M, BSA 3%, NaN_3 0.05%, sucrose 3%, sodium chloride 0.2%, phenylidextran 0.05%, bovine gammaglobulin 0.05%, pH 7.5. The binding of the carbon
15 particle conjugate to the detection zone was quantitated by measuring of absorbance (Ultrosan XL, Enhanced Laser Densitometer, LKB). IgE with standard concentrations in plasma environment (0; 0.5; 2; 10; 50, and 200 KU/L) was used as samples.

20

Results

Having four application zones for liquid and simultaneous addition, the liquids were migrating in the order of the application zones, i.e. the sample being in the zone
25 nearest to the detection zone was migrating first, without being mixed with the washing solution of the following application zone, which solution in turn started migrating, when the sample had been transported out of the application zone for samples. Correspondingly the liquids of the
30 remaining zones were migrating sequentially without being mixed.

Table 1: Analysis results from runs with sequential addition in one zone and from simultaneous addition in four
35 subzones (buffer, analytically detectable reactant, buffer, sample).

IgE KU/L	Sequential	Simultaneous
	addition in one zone (Abs x1000)	addition in 4 subzones (Abs x1000)
0,5	0	12
2	312	207
10	1241	831
50	1921	1560
200	2115	2044

In Table 1 is shown that the uptake decreases slightly for
5 strips with discrete application zones compared to when
addition is performed in one and the same zone. The
decrease is, however, marginal. Therefore the experiment
shows that generally the same result may be achieved if
simultaneous addition is performed to the zone sequence
10 LZ₄B, LZ₃R*, LZ₂B, LZ₁S as if sample, Reactant* and buffer
are added sequentially to a common application zone.

If a firmly anchored anti-IgE antibody (Reactant I) is
replaced by an allergen a determination method for IgE
15 antibodies directed to the allergen is obtained.
Analogously, test systems related to antibodies of another
class/subclass and with another specificity may be
determined. Application zones for only buffer may be
omitted. For additional alternative test protocols and
20 analytes see above under the headings "Test protocols" and
"Analytes".

EXAMPLE 2: SEQUENTIAL METHOD WITH THE ZONE SEQUENCE: LZ₄B, LZ₃R*, LZ₂B, LZ₁S, DZ. DETECTION OF hIgE IN TEST VARIANT WITH FLUORESCENT DETECTION CONJUGATE

5 Methods and materials

Coupling of anti-human IgE antibody (anti-hIgE) to a

polystyrene particle: Anti-hIgE was coupled to polystyrene particles coated with phenyldextran (prepared according to Example 1) with CDAP (1-cyano-4-dimethylaminopyridinium bromide) (Kohn J and Wilchek M, FEBS Letters 154(1) (1983) 209-210). Desalting and buffer change of anti-hIgE was performed by gel filtration (PD-10, Amersham Pharmacia Biotech AB) in NaHCO₃, 0.1 M, pH 8.5.

- 15 0.35 g of polystyrene particles (2% solution) were activated with 5.2 ml of CDAP (0.44 M) and 4.2 ml of TEA (0.2 M triethylamine, Riedel-deHaën, Germany). CDAP was added with stirring for 60 seconds and TEA for 120 seconds. A five times excess of ice-cooled deionised water was
- 20 added. The particles were centrifuged at 12,100xg (25 min., Beckman, J-21, JA-20, 10,1000 rpm). The resulting pellet was dissolved in ice-cooled, deionized water and washed once with ice-cooled deionized water and then centrifuged at 12,000 x g. 50 mg of anti-hIgE were coupled to the
- 25 activated particles (2%, 0.35 g in 0.1 M NaHCO₃, pH 8.5). Incubation with stirring was the performed for 1 hour at +4°C. After centrifugation, the particles were deactivated with glutamic acid, 0.05 M, and aspartic acid, 0.05 M in 0.1 M NaHCO₃, pH 8.5. Incubation and stirring was then
- 30 performed overnight at +4°C. Coupled particles were washed twice with 20 mM borate buffer, pH 8.5, whereupon the particle concentration was determined spectrophotometrically at A_{600nm} with untreated particles as reference. Coupled protein concentration was determined
- 35 by having radioactive anti-hIgE present during the coupling.

Coupling of anti-hIgE antibodies to detection particles:

Antibodies to hIgE cleaved with pepsin to fab'2 fragments were coupled to fluorescent polystyrene particles having aldehyde groups on their surface (Molecular Probes C-17177

- 5 TransFluoSphere, aldehyde-sulphate microspheres, 0.1 μ m, 633/720, 2% solids). 23 mg of antibody were then coupled to 66 mg of particles in 50 mM NaPO₄, pH 6.5, overnight at room temperature, whereupon 205 μ L of NaCNBH₄ (5 M) were added to reduce the coupling for 3 hours at room
- 10 temperature. Centrifugation was performed at 20,800 x g for 50 minutes (50 minutes in Eppendorf 5417R, 14,000 rpm), and deactivation in glutamic acid, 0.05 M, and aspartic acid, 0.05 M, in deionized water, pH 6.5, was then performed overnight with stirring at room temperature. After
- 15 centrifugation again at 20,800 x g, blocking was performed with 0.2% BSA in 50 mM NaPO₄, pH 7.4, with 0.05% NaN₃ and incubation was carried out overnight at +4°C. Centrifugation was then performed again at 20,800 x g and washing was performed twice with blocking buffer which was
- 20 then used also for storage. The particle concentration was determined in a fluorimeter (Perkin-Elmer LS50B) with a standard curve prepared with the original particle. Coupled protein concentration was determined by having radioactive hIgE present during the coupling.

25

Deposition of anti-hIgE-coupled particles on membrane and application zones: Was performed according to Example 1, except that the Inplastor strips were replaced by strips of adhesive tape (2 mils clear polyester Arcare with glue on

30 one side).

Test methodology: Strips with spaced application zones were mounted to an inclined plane, about 16°, in a holder. At the top (0.5 cm) of the strip (and with the detection zone

35 as the nearest zone), two sucking membranes (Whatman, 17 Chr, width 3.4 cm) were placed on top of each other. The holder also exerted a constant pressure on the sucking

membranes. For simultaneous application of reagents to the four subzones, a multichannel Finn pipette (Labsystems) was used. The multipipette was charged so that serum sample (30 μ L) was applied to the application zone nearest to the

5 detection zone in the order of buffer (15 μ L), fluorescent particle conjugate (30 μ L) and buffer (30 + 30 μ L) in the respective application zone located upstream. For sequential application to the strips without zone spacer, 30 μ L of sample were first applied to the lower end of the

10 strip. After sucking of the sample volume, buffer (15 μ L), detection particle conjugate (30 μ L) and buffer (30 + 30 μ L) were successively added after sucking. The particle conjugate was suspended in assay buffer consisting of NaPO_4 0.1 M, BSA 3 %, NaN_3 0.05 %, sucrose 10 %, NaCl, 0.15 M,

15 bovine gammaglobulin 0.05 %, pH 7.5. The measurement of time started with the application of the sample, and the time until the last buffer had been sucked into the membrane was noted. The binding of the fluorescent particle conjugate to the detection zone was quantified by scanning

20 with a red diode laser (635 ± 5 nm). As sample were used IgE standard concentrations in plasma environment (0, 0.5, 2, 10, 50 and 200 KU/L).

Results:

25 Precisely as in Example 1, the liquids migrated out of the application zone in the existing order. The time for a whole test with simultaneous application was about 20 minutes, and the time for a test with sequential

30 application was about 25 minutes.

Table 2: Analysis results from runs with sequential application in one zone and from simultaneous application in four subzones (buffer, analytically detectable reactant, buffer, sample).

KU/L	Simultaneous addition to four subzones	Sequential addition to one zone
0	0.048*	0.038*
0.5	0.053	0.047
2	0.085	0.074
10	0.286	0.256
50	1.334	1.291
200	2.507	2.487

* = scanning signal (Vmm)

Table 2 shows that the uptake is comparable for strips with
5 discrete application zones in comparison with addition to a
single zone. The experiment therefore shows that the same
result may be obtained if addition is made simultaneously
to the zone sequence LZ₄B, LZ₃R*, LZ₂B, LZ₁S as if sample,
Reactant* and buffer are added sequentially to a common
10 application zone.

EXAMPLE 3: SEQUENTIAL METHOD WITH THE ZONE SEQUENCE: LZ₅B,
LZ₄R*, LZ₃B, LZ₂S, LZ₁B, DZ. DETECTION OF BIRCH-SPECIFIC
15 hIgE IN TEST VARIANT WITH FLUORESCENT DETECTION CONJUGATE

Methods and materials

Extraction of birch pollen allergen t3, Betula verucosa: 1
part (weight) of birch pollen (Allergon, Sweden) was
20 extracted with 10 parts (volume) of 0.1 M phosphate buffer,
pH 7.4. The extraction was continued for 2 hours on a
shaker table at +4 °C. The extract was centrifuged at 4000
rpm for 1.75 hours. After filtration, the solution was
applied to a PD-10 column (Pharmacia Biotech AB) and eluted
25 in 0.1 M NaHCO₃, pH 8.5. The t3 eluate (designated: t3
extract 1/14) was taken to amino acid analysis for
determination of the total protein content..

Coupling of birch pollen allergen to polystyrene particle:

t3 extract was coupled to phenyldextran coated polystyrene particles (prepared according to Example 1) with CDAP. The coupling was effected analogously with the coupling of

5 hIgE.

Polystyrene particles (2128 mg) coated with phenyldextran in 30 % (by volume) acetone, 2 % particle suspension, were activated with 954 mg of CDAP (100 mg/ml in 30 % acetone) and 7.63 ml of 0.2 M triethylamine (TEA, Riedel-de Haen, Germany). CDAP was added with stirring and TEA was added dropwise for 90 seconds and with stirring for totally 120 seconds. The reaction was stopped by the addition of 30 % acetone (4 times the volume) and centrifugation at 12,400 g for 35 minutes. The particles were washed once with deionized water.

640 ml of t3 extract 1/14 in 0.1 M NaHCO₃, pH 8.5, were added to the activated particles, and coupling was continued for 1 hour on a shaker table. After centrifugation, the particles were deactivated with 0.05 M aspartic acid and 0.05 M glutamic acid in 0.1 M NaHCO₃, pH 8.5. Incubation then took place on a shaker table overnight at +4 °C. The particles were then washed twice with 50 mM NaPO₄, 0.05 % NaN₃, pH 7.4. The particle concentration was determined spectrophotometrically at 600 nm with uncoated polystyrene particles as reference. t3-coupled polystyrene particles were taken to amino acid analysis for determination of the total protein content.

Deposition of t3-coupled polystyrene particles on a

membrane: To nitrocellulose sheets with polyester backing (Whatman, 8 µm, 5 cm width) were applied zones of t3-coupled particles diluted to 4 % particle content in 50 mM NaPO₄, 10 % sucrose, 0.05 NaN₃, pH 7.4. The deposits were dried for 1 hour at 30 °C.

Zones for application of buffer, sample and detection

particle conjugate: Five 1 mm wide strips of adhesive tape (2 mils clear polyester, Arcare with glue on one side) were placed well separated from the zone containing the deposited material and in parallel with the zone at a distance of 5 mm from each other. The tape strips thereby defined five different 5 mm wide zones. The sheets were cut perpendicularly to the zone containing deposited material to strips having a width of 0.5 cm (the length of the strip then became 5 cm) (Singulator: Matrix 1201 membrane cutter, Kinematic automation). The final strips exhibited five zones (application zones) separated by tape strips as zone spacers and a separate zone with deposited birch pollen (detection zone). Strips without zone spacers, i.e. without separated application zones, were prepared as a comparison.

Test methodology: Strips with separated application zones were mounted, and reagents were applied as in Example 2.

Buffer (20 μ L) was applied to the zone closest to the application zone, and then serum sample (30 μ L), buffer (20 μ L), detection particle conjugate (20 μ L) and buffer (30 + 30 μ L) in the respective application zone located upstream. For sequential application to the strips without zone spacer 20 μ L of buffer were first applied to the lower end of the strip, and after sucking in thereof, 30 μ L of sample were applied in the same position and then buffer (20 μ L), fluorescent particle conjugate (20 μ L) and buffer (30 + 30 μ L). Before all applications, the preceding application had been sucked in by the strip. The detection particle conjugate and the buffer were according to Example 2.

Results:

With the application zone consisting of five subzones and with simultaneous addition thereto, it turned out that the liquids, precisely as in the Examples above, migrated out of the application zone in the existing order. The time

required for a whole test with simultaneous addition was about 21 minutes, and the time needed for a whole test with sequential addition was about 27 minutes.

- 5 **Table 3:** Analysis results from runs with sequential addition in one zone and from simultaneous addition in 4 subzones (buffer, analytically detectable reactant, buffer, sample).

	Simultaneous addition to 5 subzones	Sequential addition to 1 zone
neg	0.067*	0.058*
pos 1	1.911	2.608
pos 2	0.299	0.375

10

* = scanning signal (Vmm)

- Table 3 shows that the uptake is decreased to some extent for strips having discrete application zones compared with
15 addition to a single zone. The decrease is, however, marginal and is probably due to the fact that the flow rate in simultaneous application was somewhat delayed. The experiment therefore demonstrates that basically the same results may be achieved for simultaneous application to the
20 zone sequence LZ₅B, LZ₄R*, LZ₃B, LZ₂S, LZ₁B as if sample, Reactant* and buffer are applied sequentially to a common application zone.

CLAIMS

1. A method for determination of an analyte in a sample in a flow matrix by use of a transport flow of one or more biospecific affinity reactants, at least one of which is analytically detectable (Reactant*) and one is firmly anchored in the matrix (Reactant I), and the flow matrix comprises:
- 10 A) an application zone for liquid (LZ), containing buffer and sample and optionally one or more of the reactants, but not Reactant I,
- B) a detection zone (DZ) located downstream of LZ with the
- 15 firmly anchored reactant (Reactant I), and
- C) optionally one or more zones in which any of the reactants has been pre-deposited,
- 20 wherein (i) the flow towards the detection zone is initiated by addition of the liquid with sample in the application zone LZS for transport of analyte and reactants towards the detection zone (DZ), and (ii) the amount of Reactant* bound to DZ is detected, the detected amount
- 25 being related to the amount of analyte in the sample, characterized in that

I. the flow matrix comprises at least two application zones for liquid arranged substantially adjacent to each other:

30

$LZ_m \quad . \quad . \quad . \quad LZ_n \quad . \quad . \quad . \quad LZ_1 \quad \quad \quad DZ$
 ----->

wherein

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- a) LZ_n is an application zone for liquid, and n is the position of the application zone LZ_n ,

b) m is the total number of application zones in which flow is initiated ($m \geq 2$),

c) one LZ_n is an application zone for sample (LZ_n, S) and one LZ_n is for Reactant* (LZ_n, R^*) with $n'' \geq n'$,

d) -----> is the direction of the flow, and

e) DZ is the detection zone, and

II. flow is initiated by adding liquid to each zone $LZ_m . . . LZ_n . . . LZ_1$ in such a way that liquid _{$n+1$} , added to the application zone LZ_{n+1} , is transported through the matrix immediately after liquid _{n} , added to the nearest downstream application zone LZ_n .

2. The method according to claim 1, characterized in that $n'' > n'$ (sequential variants regarding analyte and Reactant*).

3. The method according to claim 1, characterized in that $n'' = n'$ (simultaneous variants regarding analyte and Reactant*).

4. The method according to any of the claims 1 - 3, characterized in that Reactant* is pre-deposited in its application zone (LZ_n, R^*).

5. The method according to any of the claims 1 - 4, characterized in that liquid _{$n+1$} is added to LZ_{n+1} before or substantially simultaneously with adding liquid _{n} to LZ_n , with the exception of $n = m$, which zone lacks the zone LZ_{n+1} .

6. The method according to any of the claims 1 - 5, characterized in that LZ_{n+1} finishes where LZ_n starts, with the exception of $n = m$, which zone lacks the zone LZ_{n+1} .
- 5 7. The method according to any of the claims 1 - 6, characterized in that application of liquid is performed substantially simultaneously in all $LZ_m . . . LZ_n . . . LZ_1$.
8. The method according to any of the claims 1 - 7, characterized in that $m \leq 6$; n' is 1, 2 or 3; $n' > n$; $LZ_{n'+1}$, $LZ_{n'+2}$, $LZ_{n'+3}$, $LZ_{n'-1}$, and $LZ_{n'-2}$ are application zones for liquids intended for transport of Reactant* or other reactant or buffer without reactant, as far as allowed by m , n' and n .
- 10 9. The method according to any of the claims 1 - 8, characterized in that at least one of the zones $LZ_m . . . LZ_n . . . LZ_1$ comprises a pad or material layer applied on the flow matrix.
- 15 10. The method according to any of the claims 1 - 8, characterized in that the zones $LZ_m . . . LZ_n . . . LZ_1$ have zone spacers between each other.
- 20 11. The method according to any of the claims 1 - 10, characterized in that the composition of transported components from an application zone LZ_n is not the same as from the nearest adjacent application zone LZ , in which flow is initiated, (LZ_{n+1} and LZ_{n-1} , with the exception of $n = m$ and $n = 1$, which zones lack LZ_{n+1} and LZ_{n-1} , respectively).
- 25 30 12. The method according to any of the claims 1 - 11, characterized in that at least one reactant, other than Reactant*, is pre-deposited in an application zone $LZ_{n...R}$ for liquid intended for transport of the reactant.
- 35

13. The method according to any of the claims 1 - 12, characterized in that $m \leq 6$ and that n' for the application zone for sample ($LZ_n.S$) is 1, 2 or 3.

5

14. The method according to any of the claims 1 - 13, characterized in that Reactant* has biospecific affinity for the analyte so that Reactant* is incorporated into a complex Reactant'---Analyte---Reactant* in the detection zone in an amount related to the amount of analyte in the sample, in which complex Reactant' has biospecific affinity to the analyte and is

10

(a) Reactant I, or

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(b) a reactant to which Reactant I exhibits biospecific affinity and which is transported from $LZ_n.S$ or from an application zone downstream of $LZ_n.S$.

15. The method according to any of the claims 1 - 14, characterized in that the matrix comprises at least one calibrator zone (CZ), in which calibrator is bound to, or in advance has been bound to the matrix.

16. The method according to claim 15, characterized in that the calibrator zone or zones (CZ) have a binder for the calibrator firmly anchored in the matrix, the calibrator optionally being pre-deposited in the matrix upstream of the calibrator zone or zones.

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17. The method according to any of the claims 1 - 16, characterized in that

- a. the analyte is chosen among antigens generally, and
- b. the method is performed as part of diagnosing allergy or autoimmune disease.

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18. A device for determination of an analyte in a sample in a flow matrix by use of a transport flow of one or more biospecific affinity reactants, at least one of which is analytically detectable (Reactant*) and one is firmly anchored in the matrix (Reactant I), said device comprising a flow matrix having:

- A) an application zone for liquid (LZ), containing buffer and sample and optionally one or more of the reactants, but not Reactant I,
- B) a detection zone (DZ) located downstream of LZ with the firmly anchored reactant (Reactant I), and
- C) optionally one or more zones in which any of the reactants has been pre-deposited,

characterized in that

the flow matrix comprises at least two application zones for liquid arranged substantially adjacent to each other:

LZ_m . . . LZ_n . . . LZ₁ DZ
----->

25

wherein

- a) LZ_n is an application zone for liquid, and n is the position of the application zone LZ_n,
- b) m is the total number of application zones in which flow is initiated ($m \geq 2$),
- c) one LZ_n is an application zone for sample (LZ_n,S) and one LZ_n is for Reactant* (LZ_n,R*) with $n'' \geq n'$,
- d) -----> is the direction of the flow, and

30

35

e) DZ is the detection zone.

19. The device according to claim 18, characterized in
5 that $n'' > n'$ and that the device is intended for
sequential transport of analyte and Reactant*.

20. The device according to claim 18, characterized in
that $n'' = n'$ and that the device is intended for
10 simultaneous transport of analyte and Reactant*.

21 The device according to any of the claims 18 - 20,
characterized in that Reactant* is pre-deposited in its
application zone ($LZ_{n''}R^*$).
15

22. The device according to any of the claims 18 - 21,
characterized in that LZ_{n+1} finishes where LZ_n starts, with
the exception of $n = m$, which zone lacks the zone LZ_{n+1} .

20 23. The device according to any of the claims 18 - 22,
characterized in that $m \leq 6$; n' is 1, 2 or 3; $n'' > n'$;
 $LZ_{n'+1}$, $LZ_{n'+2}$, $LZ_{n'+3}$, $LZ_{n'-1}$, and $LZ_{n'-2}$ are application zones
for liquids intended for transport of Reactant* or other
reactant or buffer without reactant, as far as allowed by
25 m , n'' and n' .

24. The device according to any of the claims 18 - 23,
characterized in that the zones LZ_m . LZ_n . LZ_1 have
zone spacers between each other.
30

25. The device according to any of the claims 18 - 23,
characterized in that at least one of the zones
 LZ_m . LZ_n . LZ_1 comprises a pad or material layer
applied on the flow matrix.
35

26. The device according to any of the claims 18 - 25, **characterized** in that at least one reactant, other than Reactant*, is pre-deposited in an application zone $LZ_n...R$ for liquid intended for transport of the reactant.

5

27. The device according to any of the claims 18 - 26, **characterized** in that $m \leq 6$ and that n' for the application zone for sample ($LZ_n.S$) is 1, 2 or 3.

10 28. The device according to any of the claims 18 - 27, **characterized** in that the detection zone DZ comprises firmly anchored Reactant I, and that a reactant to which Reactant I exhibits biospecific affinity optionally is pre-deposited in $LZ_n.S$ or in an application zone downstream of
15 $LZ_n.S$.

29. The device according to any of the claims 18 - 28, **characterized** in that the flow matrix comprises at least one calibrator zone CZ, in which a calibrator or a binder
20 for the calibrator is firmly anchored in the matrix.

30. The device according to claim 29, **characterized** in that the calibrator zone or zones (CZ) have a binder for the calibrator firmly anchored in the matrix, and that
25 calibrator optionally is pre-deposited in the matrix upstream of the calibrator zone or zones.

31. The device according to any of the claims 18 - 30, **characterized** in that the device is intended for diagnosing
30 allergy or autoimmune disease.

32. A test kit, **characterized** in that the kit comprises (i) a device according to any of claims 18 - 29 and (ii) Reactant*.

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33. The test kit according to claim 32, characterized in that the kit additionally comprises (iii) a calibrator when a binder for the calibrator is firmly anchored in the matrix.

INTERNATIONAL SEARCH REPORT

International application No.

PCT/SE 98/02463

A. CLASSIFICATION OF SUBJECT MATTER

IPC6: G01N 33/53

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC6: G01N

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

SE,DK,FI,NO classes as above

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

WPI, EPODOC, TXTE

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	EP 0306336 A2 (SYNTEX (U.S.A.) INC.), 8 March 1989 (08.03.89), See esp. column 20, line 64 - column 22, line 61 --	1-33
A	WO 9202818 A1 (PURDUE RESEARCH FOUNDATION), 20 February 1992 (20.02.92) --	1-33
A	WO 9114942 A1 (PACIFIC BIOTECH, INC.), 3 October 1991 (03.10.91) -- -----	1-33

☐ Further documents are listed in the continuation of Box C.
 ☒ See patent family annex.

* Special categories of cited documents:

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier document but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance: the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance: the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

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INTERNATIONAL SEARCH REPORT

Information on patent family members

02/03/99

International application No.

PCT/SE 98/02463

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